



Available online at www.sciencedirect.com





Asia-Pacific Journal of Sports Medicine, Arthroscopy, Rehabilitation and Technology 2 (2015) 114–121 www.ap-smart.com

Review article

# Review of ankle inversion sprain simulators in the biomechanics laboratory

# Sophia Chui-Wai Ha<sup>a</sup>, Daniel Tik-Pui Fong<sup>b</sup>, Kai-Ming Chan<sup>a,\*</sup>

<sup>a</sup> Department of Orthopaedics and Traumatology, Prince of Wales Hospital, Faculty of Medicine, The Chinese University of Hong Kong, Hong Kong

<sup>b</sup> National Centre for Sport and Exercise Medicine, School of Sport, Exercise and Health Sciences, Loughborough University, Loughborough, Leicestershire, United Kingdom

> Received 28 March 2014; revised 7 August 2015; accepted 27 August 2015 Available online 21 October 2015

#### Abstract

Ankle inversion ligamentous sprain is one of the most common sports injuries. The most direct way is to investigate real injury incidents, but it is unethical and impossible to replicate on test participants. Simulators including tilt platforms, trapdoors, and fulcrum devices were designed to mimic ankle inversion movements in laboratories. Inversion angle was the only element considered in early designs; however, an ankle sprain is composed of inversion and plantarflexion in clinical observations. Inversion velocity is another parameter that increased the reality of simulation. This review summarised the simulators, and aimed to compare and contrast their features and settings.

Copyright © 2015 Asia Pacific Knee, Arthroscopy and Sports Medicine Society. Published by Elsevier (Singapore) Pte Ltd. This is an open access article under the CC BY-NC-ND license (http://creativecommons.org/licenses/by-nc-nd/4.0/).

Keywords: ankle biomechanics; ankle injuries; inversion; sprain simulation

#### Introduction

Ankle inversion ligamentous sprain is very common in sports. It accounts for > 80% of all ankle injuries, and the recurrence rate is as high as 80%.<sup>1</sup> Individuals having recurrent ankle sprains are highly susceptible to chronic ankle instability and stiffness.<sup>2</sup> Extensive clinical and basic science research on this injury has been conducted.<sup>3–5</sup> The ankle complex consists of three articulations: the talocrural joint, the subtalar joint, and the distal tibiofibular syndesmosis. These joints allow the rearfoot to move as a single unit in multiplanes rather than in one single plane.<sup>6</sup> Most of the ankle injuries take place during jump landing<sup>7</sup> when the foot is inverted and plantarflexed,<sup>8</sup> also known as supination.<sup>9</sup>

Excessive supination can damage the lateral ligament complex structure. Three main ligaments are found in this complex: the anterior talofibular ligament, the posterior

E-mail address: kaimingchan@cuhk.edu.hk (K.-M. Chan).

talofibular ligament, and the calcaneofibular ligament. Among these three ligaments, the anterior talofibular ligament is most vulnerable because it bears the greatest strain when the foot undergoes plantarflexion.<sup>10</sup> It has the lowest ultimate load of 138.9 N,<sup>11</sup> which makes it the first ligament to be injured in inversion sprain cases.<sup>12</sup>

Various approaches were reported in the literature to understand the injury mechanism quantitatively. The biomechanics of ankle supination sprain was first evaluated in cadaver studies.<sup>13–15</sup> The computational forward dynamic method was performed to determine the influence of foot position at touchdown on ankle sprain susceptibility by simulating side-shuffle movement kinematics.<sup>16</sup> Injuries were captured by calibrated motion analysis equipment in biomechanics laboratories occasionally. Three injury case reports with kinematics data have been published recently.<sup>17–19</sup>

The most direct way to study injury mechanism is to investigate real incidents; however, it is impossible and unethical to perform experiments that are intentionally hurting the test participants. To study ankle inversion sprain movements in calibrated environment, subinjury trials could be carried out with the assistance of tilt platforms, trapdoors, and fulcrum

http://dx.doi.org/10.1016/j.asmart.2015.08.002

<sup>\*</sup> Corresponding author. Department of Orthopaedics and Traumatology, Prince of Wales Hospital, Faculty of Medicine, The Chinese University of Hong Kong, Hong Kong.

<sup>2214-6873/</sup>Copyright © 2015 Asia Pacific Knee, Arthroscopy and Sports Medicine Society. Published by Elsevier (Singapore) Pte Ltd. This is an open access article under the CC BY-NC-ND license (http://creativecommons.org/licenses/by-nc-nd/4.0/).

devices. This review provides information on the existing ankle inversion simulators. In addition, it compares and contrasts their features in terms of their inversion angles, inversion velocities, supination angles, and appearance (see Table 1).

#### Materials and methods

A systematic search of AMED, Embase (via OvidSP), MEDLINE, and SPORTDiscus was conducted from the earliest archives to the last week of December 2013. The keyword string used for search was "ankle AND (inversion sprain\* OR inversion injur\* OR sprain\* OR strain\* OR instabilit\* OR ankle instabilit\* OR chronic instabilit\* OR joint instabilit\* OR mechanical instabilit\* OR functional instabilit\* OR perceived instabilit\* OR subjective instabilit\* OR unstab\* OR lax\* OR giv\* way) AND (sudden fall OR standing ankle inversion OR perturbation OR supinati\* platform OR tilt\* platform OR simulati\* inversion OR simulati\* platform OR fulcrum) AND (lab\* OR biomechanic\* lab\*)", which

Table 1		
Categorisations of trapdoors, tilt platforms,	and fulcrum	devices.

Appearance	Reference
Trapdoor or tilt platform	Sprigings et al <sup>20</sup>
	Nawoczenski et al <sup>21</sup>
	Johnson & Johnson <sup>22</sup>
	Lynch et al <sup>23</sup>
	Podzielny & Hennig <sup>24</sup>
	Vaes et $al^{25,26}$
	Anderson et al <sup>32</sup>
	Chan et al <sup>34</sup>
	Cordova et al <sup>35</sup>
	Cordova & Ingersoll <sup>36</sup>
	Ebig et al <sup>37</sup>
	Eechaute et al <sup>38</sup>
	Eechaute et al <sup>39</sup>
	Eils & Rosenbaum <sup>40</sup>
	Grüneberg et al <sup>41</sup>
	Isakov et al <sup>43</sup>
	Karlsson & Andreasson <sup>44</sup>
	Kimura et al <sup>45</sup>
	Konradsen & Ravn <sup>46</sup>
	Konradsen et al <sup>47</sup>
	Lofvenberg et al <sup>48</sup>
	Lohrer et al <sup>49</sup>
	Myers et al <sup>50</sup>
	Nieuwenhuijzen et al <sup>51</sup>
	Osborne et al <sup>52</sup>
	Pederson et al <sup>54</sup>
	Ricard et al <sup>55,56</sup>
	Scheuffelen et al <sup>58</sup>
	Schmitt et al <sup>59</sup>
	Sheth et $al^{60}$
	Shima et al <sup>61</sup>
	Zhang et al <sup>64</sup>
Runway	McLoda & Hansen <sup>29</sup>
	Nieuwenhuiizen et al <sup>51</sup>
	Ty Hopkins et $al^{62}$
Fulcrum	Ubell et al <sup>27</sup>
Fulcium	Ashton-Miller et al <sup>28</sup>
	Knight & Weimer <sup>31</sup>
	Anderson et al <sup>32</sup>
	Ottaviani et al $^{53}$

appeared in the title, abstract, or keyword fields. The initial total number of articles in the database was 259. Results were first screened by reading the title and abstract. Nonrelevant articles were eliminated and the count was reduced to 80. Reference lists of the selected published journals were screened to retrieve additional studies. Duplicates, non-English articles, animal studies, and nonrelevant reports were excluded. Full texts of articles were obtained from the university library system. Data related to inversion angle, inversion velocity, supination angle, and appearance of the instrument were extracted. After the screening process, the final number of articles included in this review was 46.

#### Results

In this review, 46 journal articles about tilt platforms, trapdoors, and dynamic fulcrum devices, published during 1981–2012, were included.<sup>20–64</sup> Researchers have employed these instrument to perform motion tasks, including standing, step down, jump landing, and walking, in order to determine internal and external effects on simulated sprain conditions.<sup>21–26,28,32–39,41,46–52,54–64</sup> Internal aspects including muscle activation and sensorimotor influences, and external protectors such as taping and bracing were evaluated. Besides, the effects of training intervention were assessed. These simulators mimic incorrect landing postures, inversion or supination, which are susceptible to inversion sprain injury. The aim of this review is to summarise all reported sprain simulators in terms of their inversion angles, inversion velocities, supination angles, and appearances.

#### Discussion

#### Inversion angles

The first study that employed a tilt platform was conducted by Sprigings et al.<sup>20</sup> The inversion angles generated by all reported trapdoors, tilt platforms, and fulcrums ranged from  $15^{\circ}$  to  $50^{\circ}$  (see Table 2).<sup>20-64</sup> A real injury may take place if the inversion angle exceeds  $35^{\circ}$ .<sup>21,22</sup> An inversion of  $35^{\circ}$  was recorded in an accident that occurred in the laboratory,<sup>18</sup> compared to an inversion of  $48^{\circ}$  in an international competition.<sup>65</sup> The injury severity depends on the intensity of a motion. Most of the simulators could produce <  $30^{\circ}$  inversion tilt, which was safe and ethical. However, Vaes and coworkers<sup>25,26</sup> had developed a platform that could generate a unilateral inversion at  $50^{\circ}$  from a risky preparation of plantarflexing at  $40^{\circ}$  and internally rotated at  $15^{\circ}$ . Researchers claimed that the  $50^{\circ}$  simulation was completely harmless. No conclusion could be made on the minimum inversion angle causing an ankle lateral ligamentous sprain.

#### Inversion velocities

Based on the fact that speed contributes to the injury severity, Lynch and colleagues<sup>23</sup> were the first to use a tilt platform that had two kinematic controls to investigate if uninjured participants showed muscles latency. The platform could give an

## sina-pub.ir

116

# Table 2 Inversion angle of all ankle sprain simulators, including trapdoors, tilt platforms, and fulcrum devices.<sup>a</sup>

Authors	Inversion (°)	Appearance
Isakov et al <sup>43</sup>	20	A special apparatus that enables generation of sudden inversion. One rotating platform with a
		fixed platform was used.
Sheth et al <sup>60</sup>	20	A customised platform; one-half of the platform has a hinged trapdoor that can produce 20° of
Osborne et $al^{52}$	20	inversion, while another half was a scale ensuring 20% weight bearing of the foot.
Anderson et al <sup>32</sup>	22	A wooden tilt platform with a tiltable surface used to invert one foot; the participant had to position the entire body weight on the right foot placed on the tiltable surface.
Ubell et al <sup>27</sup>	24	The fulcrum was 27 mm high & caused a maximum shoe sole inversion of 24° when the outer edge of the shoe sole touched down on a hard, level support surface.
Grüneberg et al <sup>41</sup>	25	A landing surface consists of a box with a trandoor for the left foot and the box for the right
		foot is in the same dimension and material. A resistance of 200 g is needed for the first visible restriction $\frac{1}{2}$ , 2200 a for a rate tion of 25°
Shima at $a1^{61}$	25	Foldholf & 2500 g for a foldholf of 25. A transformed at an angle of $25^\circ$ with the horizontal plane. A participant
	25	was instructed to place one foot on the platform & rest the other foot on another platform of the same size & height. The space between the feet was $\sim 20$ cm. We instructed the
		participants to have their body weight distributed equally on both feet.
Knight & Weimar <sup>30</sup>	25	A fulcrum sole, 6 mm thick & 30 mm high, was placed at 20 mm from the medial
Knight & Weimar <sup>31</sup>	25	border & ran the length of the outer sole; it could generate 25° of inversion.
Sprigings et al <sup>20</sup>	30	An ankle inverter platform consisted of a raised platform, which had a hinged trapdoor built into it. The trapdoor could be manually activated to collapse at an angle of $30^{\circ}$ below the
		horizontal. Approximately 2 N force was needed for the trapdoor to collapse.
Konradsen & Ravn <sup>46</sup> Konradsen et al <sup>47</sup>	30	A trapdoor capable of tilting to $30^{\circ}$ in the frontal plane. Weight was evenly distributed on 2 feet.
Karlsson & Andreasson <sup>44</sup>	30	A manual activation ankle inverting platform with a trapdoor mechanism. Two platforms
		were placed 25 cm apart, allowing the participant to distribute body weight equally on both plates.
Lofvenberg et al <sup>48</sup>	30	A hinge trapdoor with two movable platforms that could be tilted to 30° in the frontal plane.
		The platform was released by an electrically powered motor.
Eils & Rosenbaum <sup>40</sup>	30	Custom-designed ankle inversion platform, with both feet being fixed on independently
		movable trapdoors. Each footplate was positioned at 40° PF, with the shoe at 15° of
		adduction. The operator then imposed a sudden 50° of inversion.
Nieuwenhuijzen et al <sup>31</sup>	30	A mechanically induced trapdoor box, which was 35 cm long, 20 cm wide, & 10 cm high. A spiral spring kept the trapdoor on top of the box in neutral position. A resistance of 200 g
50		was needed to tilt the door to $0.1^{\circ}$ & 2300 g for ° rotation. The trapdoor could tilt up to 30°.
Myers et al	30	An ankle inversion perturbation device allowed the ankle joint to drop from a neutral position to 30° inversion when the participant was standing. The inversion velocity was ~440°/s. The participant was instantiated to assume again which distribution between the 2 limbs.
Ty Hopkins et $al^{62}$	30	A transform mechanism built into a runway was used for the walking trials. The runway
Ty Hopkins et al	50	consisted of five 1.22 m interchangeable segments with the trandoor mechanism incorporated
		into 1 segment.
Chan et al <sup>34</sup>	30	A pair of supination sprain simulators consisted of an L-shaped supporting frame, which was
		0.34 m wide & 0.25 m high. A rotating disc on top of the platform allowed angle adjustment.
Zhang et al <sup>64</sup>	30	A custom-built trapdoor inversion platform could invert the ankle to 30°.
Scheuffelen et al <sup>58</sup>	20/30	A tilt platform could generate either 20° or 30° of inversion.
Kimura et al <sup>45</sup>	35	A 35° inversion platform allowed for a comfortable stance position & a normal base of
Nawoczenski et al <sup>21</sup>		support. A ledge was placed on the lateral side to prevent foot slippage.
Johnson & Johnson <sup>22</sup>	35	An electrically released special apparatus could produce inversion of either ankle. A solenoid
		was placed on either side of the apparatus to control foot-plate release mechanism. An
		adjustable sidebar was put laterally to block the foot.
Pederson et al <sup>54</sup>	35	An inversion platform that could produce 35° of inversion. The participant was instructed to
		balance on right foot by putting all the weight on the right side.
Cordova et al <sup>35</sup>	35	A custom-made inversion platform to produce inversion movement.
Cordova & Ingersoll <sup>36</sup>		
Ricard et al <sup>33,30</sup>	35	An inversion platform with a foot-support base that rotated by 35° after a trapdoor was
		released. A side bar on the right platform was used to ensure shoe position. The participants
		were instructed to put all their weight on the right foot, using the toes of the left foot to
139		maintain balance, before & after the dropping of platform.
Eechaute et al	Preparation:	Custom-designed ankle inversion platform, with both feet fixed on independently movable
	40° PF & 15° adduction	trapdoors. Each tootplate was positioned at $40^{\circ}$ plantarflexion, with the shoe at $15^{\circ}$ of
	50° IV	adduction. Operator then imposed a sudden 50° of inversion.

PF = plantar flexion; IV = inversion.

<sup>a</sup> The devices are in ascending order with respect to the inversion angle.

inversion of 18° at a peak velocity of 446°/s. Study participants needed to prepare themselves in neutral position or plantarflexing their ankles in 20°. The inversion velocity could be controlled to either 50°/s or 200°/s. Four scenarios were simulated: 0° plantarflexion at 50°/s, 20° plantarflexion at 50°/s, 0° plantarflexion at 200°/s, and 20° plantarflexion at 200°/s. This allowed simulation at different intensities by varied combinations of ankle movements at different speed. Two other

binations of ankle movements at different speed. Two other studies measured the inversion velocities when testing. The platform used by Ricard et al<sup>55</sup> could produce a speed of up to  $517^{\circ}$ /s. Knight and Weimar<sup>30</sup> introduced a fulcrum device, which could generate velocities in the range of  $573-625^{\circ}$ /s. This range of speed is similar to the intensity of the injury that occurred in international competition.<sup>65</sup>

#### Supination angles

Wright et al<sup>16</sup> proposed that touchdown plantarflexion increases the occurrences of an ankle inversion sprain. A plantarflexed ankle refers to a foot contacting the ground with the toes or forefoot. This motion increases the moment arm among the subtalar joint axis and thus the joint torque, followed by a sudden explosive twisting motion, and thus an ankle inversion sprain occurs.<sup>66</sup> Simulators that can initiate multiplane motion allow us to have a better understanding of ankle supination sprain kinematics (see Table 3).

Several platforms needed the participants to be at a plantarflexed position before the unexpected tilting.<sup>23,25,26</sup> The participants were at high risk and unstable positions; thus, these platforms could narrow the gap between subinjury trials and injury cases.

The ankle consists of the talocrural joint and the subtalar joint.<sup>1</sup> When these two joints work together, the ankle could either supinate or pronate. The suggested ankle sprain injury mechanism was inversion, plantarflexion, and internal rotation.<sup>9</sup> Every sprain motion is different, and does not occur only on one single plane purely but is accompanied by the other two planes.<sup>34</sup> The most flexible simulators were developed by Chan et al<sup>34</sup> (Figure 1A and B). A rotating disc was added on top of the platforms; different supination situations could be simulated accordingly (see Figure 2A and B). They reported ankle kinematics when the ankle was forced to have pure inversion of 30°; supination of 23°, 45°, and 67°; and pure plantarflexion. The study design and device were approved by Joint Chinese University of Hong Kong-New Territories East Cluster Clinical Research Ethics Committee.

#### Tilt platform in runway

Ankle sprains occur in dynamic situations, including walking, running, inappropriate jump landing, and stepping on uneven surfaces, rather than in standing situation, with both feet bearing the weight. Ankle sprain mostly occurred during systematic loading and unloading, but not when the ankle was fully loaded because of the anatomical restraints.<sup>67</sup> Nieuwenhuijzen and colleagues<sup>51</sup> put a trapdoor box on a treadmill. The left ankle of the study participants might invert when walking. A velocity of 403°/s was measured, which is close to

Table 3

Supination angle of all ankle sprain simulators, including trapdoors, tilt platforms, and fulcrum devices.

Author	Supination	Appearance
Ottaviani et al <sup>53</sup>	15° IV &	A specially designed testing apparatus forced the right ankle of each participant to
Ashton-Miller et al <sup>28</sup>	0° or 16° or 32° PF	invert 15° at 0°, 16°, 32° of plantarflexion. The apparatus consisted of a shoe securely fastened to a 1.5 cm thick $36 \times 20$ cm <sup>2</sup> board, with a track accommodating a 40 cm long $5 \times 10$ mm <sup>2</sup> steel bar underneath.
Lynch et al <sup>23</sup>	Preparation at 0° or 20° PF	A tilt platform achieved a tilt by a hydraulic activator. Velocity & magnitude could be adjusted. Preparation position could be either at neutral or at 20° of plantarflexion. The velocity could also be adjusted to 50°/s or 200°/s
Podzielny & Henning <sup>24</sup>	26° sideway 13° PF	A metal platform with foot plantarflexion, adduction, & inversion motions. A special release mechanism could drop the right platform to an angle of 26° sideways & 13° of plantarflexion. The abduction angle of the foot during standing was 23°. The left platform was used for balancing.
Lohrer et al <sup>49</sup>	30° IV & 15° PF	An inversion tilt platform induced 30° of inversion & $15^{\circ}$ of plantarflexion. The participant was instructed to put 90% of body weight on the right foot.
Ricard et al <sup>55,56</sup>	37° IV & 15° PF	An inversion platform with a foot-support base that rotated 37° after a trapdoor was released. To help simulate the mechanism of sprain, the back of the inversion platform was raised to allow the subject to be tested at 15° of plantar flexion. The participant was asked to balance on the right side.
Chan et al <sup>34</sup>	Pure IV to pure PF	A pair of supination sprain simulators consisted of an L-shaped supporting frame(0.34 m wide & 0.25 m high). A rotating disc on top of the platform allowed angle adjustment.
Schmitt et al <sup>59</sup>	$30^{\circ}$ IV & $15^{\circ}$ PF & $24^{\circ}$ supination	A custom-made tilting platform allowed simulation of an inversion movement of 30° of effective perturbation angle. The built-in rotation axis permitted solely an inversion movement composed of a 15° of plantarflexion & a 24° supination movement.
Vaes et al <sup>25,26</sup>	Preparation at 40° PF & 15° adduction	A sprain simulation platform needed participants to place their right foot fixed on a
Eechaute et al <sup>38</sup>	50° inversion	rotation pulley & the ankle was at 40° of plantarflexion & 15° of adduction. The foot & ankle were stressed in inversion using a 15 kg load that internally rotated the pulley.

PF = plantarflexion; IV = inversion.

### sina-pub.ir

118

S.C.-W. Ha et al. / Asia-Pacific Journal of Sports Medicine, Arthroscopy, Rehabilitation and Technology 2 (2015) 114-121



Figure 1. (A) A participant, in preparation, standing on the tilt platforms. (B) The right platform was tilted at  $30^{\circ}$ , forcing the participant to invert the right ankle. *Note*. Ankle inversion simulator was fabricated by Chan et al.<sup>34</sup>

the real injury inversion velocity. The participants might expect an inversion in this test, as the only trapdoor on the left was placed on the treadmill.

McLoda and Hansen<sup>29</sup> put an inversion platform in a runway. Five interchangeable segments were placed in the runway, one of them being an inversion platform. Researchers randomly placed the platforms in one of the segments. Either the left or the right ankle of the study participants might be tested when walking. A pressure of 0.45 kg applied to the platform could trigger the inversion of the platform.

#### Fulcrum sole

Ankle sprains rarely occur in a person with equal weight distribution on both feet. The fulcrum device was developed by Ubell et al.<sup>27</sup> It is a device that generates inversion speed by participants' weight instead of depending on the mechanical tilt. An unexpected inversion experiment was performed by using either a flat dummy sole or a fulcrum sole to simulate foot inversion movement. A fulcrum, 27 mm high and 6 mm wide, was attached to a sole at 20 mm medial to the midline. This could increase the rapidity and magnitude of simulation. The ankle ligaments might exceed the stretching tolerance if the subtalar joint inverts more than  $30^{\circ}$ .<sup>28</sup> Therefore, the inversion



Figure 2. (A) A participant in preparation standing in the middle of the tilt platforms. Frames of both platforms were rotated to generate a combination of inversion and plantarflexion. (B) The participant was forced to supinate the right ankle. Frames of both platforms were rotated to generate a combination of inversion and plantarflexion. *Note*. Ankle inversion simulator was fabricated by Chan et al.<sup>34</sup>

angle produced by this fulcrum sole design was limited to 24°. Either a flat dummy sole or a fulcrum sole was attached to the shoe when the participant was seated with their eyes closed.

Another fulcrum sole was developed by Knight and Weimar<sup>30,31</sup> based on Ubell et al's<sup>27</sup> design. They used a similar fulcrum, which was 30 mm high, 6 mm thick, placed 20 mm from the medial border, and was of the same length as that of the outer sole. This fulcrum could produce a 25° inversion. The sole with fulcrum was 0.178 kg, while the flat one weighed 0.134 kg. Both had similar weights in order to prevent estimation. The participants were instructed to step down on a metal surface from a high block. The inversion velocity was calculated during data processing. The sole could reach a speed of 625°/s for an injured ankle and 573°/s for an uninjured ankle. Compared to the slowest inversion velocity (632°/ s) recorded in a real tennis match,<sup>68</sup> this fulcrum device could produce a very-close-to-injury scenario. Table 4

1	1	0
L	1	7

Authors	Inversion (°)	Inversion velocity	Appearance
Lynch et al <sup>23</sup>	18	50°/s or 200°/s (controlled)	A tilt platform achieved a tilt by a hydraulic activator. Velocity & magnitude could be adjusted. Preparation position could be either at neutral or $20^{\circ}$ of plantarflexion.
Ricard et al <sup>55,56</sup>	37	Up to 517°/s in measurement	The velocity could also be adjusted to $50$ /s or 200 /s. An inversion platform with a foot-support base that rotated $37^{\circ}$ after a trapdoor was released. To help simulate the mechanism of sprain, the back of the inversion platform was released to allow the which to be tasted at $15^{\circ}$ of planter flavion. The
Nieuwenhuijzen et al <sup>51</sup>	30	Walking: 403°/s Jumping: 595°/s	subject was asked to allow the subject to be tested at 15° of plantar nexton. The subject was asked to balance on the right side. A mechanically induced trapdoor box, which was 35 cm long, 20 cm wide, & 10 cm high. A spiral spring kept the trapdoor on top of the box in neutral position. A resistance of 200 g was needed to tilt the door to 0.1° & 2300 g for a rotation of
Knight & Weimar <sup>30</sup>	25	573-625°/s in measurement	25°. The trapdoor could tilt up to 30°. A fulcrum sole, 6 mm thick & 30 mm high, was placed at 20 mm from the medial border & ran the length of the outer sole: it could generate 25° of inversion

Inversion velocity of all ankle sprain simulators, including trapdoors, tilt platforms, and fulcrum devices.<sup>a</sup>

<sup>a</sup> The devices are in ascending order with respect to the inversion velocity.

### Conclusion

Biomechanical researchers have been using trapdoors and tilt platforms to simulate ankle inversion motion in laboratories to study inversion sprain injury mechanism. These tools had different settings and appearances. The objectives of included passive tests studying the latency,<sup>20–23,25,26,29,31,33</sup> -3840 - 444648peroneal and investigating the effect of bracexternal ankle taping,<sup>28,31,49,54,55,61</sup> 28,32,34,35,42,43,55,58,60 ings.<sup>20,24,25,2</sup> the effects of training interventions,<sup>40,52,60</sup> and sensorimotor influence of the lateral ankle ligaments.<sup>40,42,49,50</sup> Trapdoors were also being placed in runways to perform walking tests.<sup>50,51,62</sup> Fulcrum removable sole was another design which attached beneath the shoes. Researchers would put a fulcrum sole or a dummy sole beneath participants' shoes before performing jump-landing and step-down tasks as these motions are prone to ankle inversion sprains in sport events.<sup>30,31</sup> These tools allowed researchers to understand the injury mechanism and causes of injury, and thus to improve the existing preventive appliances. Inversion angle was being seen as the only motion in early designs, but ankle sprain is not a single-plane motion. All tilt platforms and fulcrum devices included in this article were reported to show a tilt range of 15-50°. Inversion speed can affect the severity of injury, as our peroneal muscles cannot respond fast enough in order to correct the ankle orientation. Therefore, researchers started to control the inversion velocity of simulators to a more realistic situation. The inversion velocities ranged from 50°/s to over  $600^{\circ}$ /s (see Table 4). Some platforms were able to produce multiplane motions, including supination or plantarflexion, to simulate the motion to a more realistic extent.

The major limitations of studying sports injury in biomechanics laboratories are safety and ethical issues. All simulators have their strengths and weaknesses. To simulate an injury close to reality, motions including walking, jump-landing, and step-down tasks are highly recommended. Both supination angle and velocity should be considered when developing a simulator.

#### Summaries of this review

- (1) Ankle inversion ligamentous sprain is very common in sports events but rare in laboratories. It is unethical and impractical to sprain living persons' ankles intentionally.<sup>65</sup> Trapdoors, tilt platforms, and fulcrum devices were fabricated to mimic the sprain motion in laboratories.
- (2) A supinating platform consisting of both inversion and plantarflexion motions would be a better option for researchers to study ankle supination sprains.
- (3) Inversion velocity contributes to the ankle inversion sprain injury. In order to produce a close-to-injury velocity in a laboratory on test participants, researchers may consider using the weight of the participants to generate the speed instead of depending on the machine to do so.

#### **Conflicts of interest**

The authors have no conflicts of interest relevant to this article.

#### **Funding/support**

There were no sources of funding for the work described in this manuscript.

#### References

- Fong DTP, Hong Y, Chan LK, Yung PSH, Chan KM. A systematic review on ankle injury and ankle sprain in sports. *Sports Med.* 2007;37:73–94.
- Freeman MA, Dean MR, Hanham IW. The etiology and prevention of functional instability of the foot. J Bone Joint Surg Br. 1965;47:678–685.
- Smith RW, Reischl SF. Treatment of ankle sprains in young athletes. Am J Sports Med. 1986;14:465–471.
- Yeung MS, Chan K, So CH, Yuan WY. An epidemiological survey on ankle sprain. Br J Sports Med. 1994;28:112–116.
- Hertel J. Functional instability following lateral ankle sprain. Sports Med. 2000;29:661–671.
- Hertel J. Functional anatomy, pathomechanics, and pathophysiology of lateral ankle instability. J Athl Train. 2002;37:364–375.

### sina-pub.ir

120

- 7. Dufek JS, Bates BT. Biomechanical factors associated with injury during landing in jump sports. *Sports Med.* 1991;12:326–337.
- 8. Garrick JG. The frequency of injury mechanism of injury, and epidemiology of ankle sprains. *Am J Sports Med.* 1977;5:241-242.
- **9.** Safran MR, Benedetti RS, Bartolozzi 3rd AR, Mandelbaum BR. Lateral ankle sprains: a comprehensive review: part 1: etiology, pathoanatomy, histopathogenesis, and diagnosis. *Med Sci Sports Exerc.* 1999;31:S429–S437.
- Bennett WF. Lateral ankle sprains. Part I: anatomy, biomechanics, diagnosis, and natural history. *Orthop Rev.* 1994;23:381–387.
- Attarian DE, McCrackin HJ, DeVito DP, McElhaney JE, Garrett WE. A biomechanical study of human ankle ligaments and autogenous reconstructive grafts. *Am J Sports Med.* 1985;13:377–381.
- Fong DTP, Wei F, Hong Y, Krosshaug T, Haut RC, Chan KM. Ankle ligament strain during supination sprain injury—a computational biomechanics study. *Port J Sport Sci.* 2011;11:655–658.
- 13. Markolf KL, Schmalzried TP, Ferkel RD. Torsional strength of the ankle *in vitro*. The supination-external-rotation injury. *Clin Orthop Relat Res*. 1989:266–272.
- Self BP, Harris S, Greenwald RM. Ankle biomechanics during impact landings on uneven surfaces. *Foot Ankle Int.* 2000;21:38–144.
- Self BP, Paine D. Ankle biomechanics during four landing techniques. Med Sci Sports Exerc. 2001;33:1338–1344.
- Wright IC, Neptune RR, van den Bogert AJ, Nigg BM. The influence of foot positioning on ankle sprains. J Biomech. 2000;33:513–519.
- 17. Fong DTP, Hong Y, Shima Y, Krosshaug T, Yung PSH, Chan KM. Biomechanics of supination ankle sprain: a case report of an accidental injury event in the laboratory. *Am J Sports Med.* 2009;37:822–827.
- Kristianslund E, Bahr R, Krosshaug T. Kinematics and kinetics of an accidental lateral ankle sprain. J Biomech. 2011;44:2576–2578.
- **19.** Gehring D, Wissler S, Mornieux G, Gollhofer A. How to sprain your ankle—a biomechanical case report of an inversion trauma. *J Biomech*. 2013;46:175–178.
- Sprigings EJ, Pelton JD, Brandell BR. An EMG analysis of the effectiveness of external ankle support during sudden ankle inversion. *Can J Appl Sport Sci.* 1981;6:72–75.
- Nawoczenski DA, Owen MG, Ecker ML, Altman B, Epler M. Objective evaluation of peroneal response to sudden inversion stress. J Orthop Sports Phys Ther. 1985;7:107–109.
- Johnson MB, Johnson CL. Electromyographic response of peroneal muscles in surgical and nonsurgical injured ankles during sudden inversion. J Orthop Sports Phys Ther. 1993;18:497–501.
- Lynch SA, Eklund U, Gottlieb D, Renstrom PA, Beynnon B. Electromyographic latency changes in the ankle musculature during inversion moments. *Am J Sports Med.* 1996;24:362–369.
- 24. Podzielny S, Hennig EM. Restriction of foot supination by ankle braces in sudden fall situations. *Clin Biomech*. 1997;12:253–258.
- 25. Vaes P, Duquet W, Casteleyn PP, Handelberg F, Opdecam P. Static and dynamic roentgenographic analysis of ankle stability in braced and nonbraced stable and functionally unstable ankles. *Am J Sports Med.* 1998;26:692–702.
- **26.** Vaes P, Duquet W, Gheluwe BV. Peroneal reaction times and eversion motor response in healthy and unstable ankles. *J Athl Train.* 2002;37:475–480.
- Ubell ML, Boylan JP, Ashton-Miller JA, Wojtys EM. The effect of ankle braces on the prevention of dynamic forced ankle inversion. *Am J Sports Med.* 2003;31:935–940.
- 28. Ashton-Miller JA, Ottaviani RA, Hutchinson C, Wojtys EM. What best protects the inverted weightbearing ankle against further inversion? Evertor muscle strength compares favorably with shoe height, athletic tape, and three orthoses. *Am J Sports Med.* 1996;24:800–809.
- McLoda TA, Hansen AJ. Effects of a task failure exercise on the peroneus longus and brevis during perturbed gait. *Electromyogr Clin Neurophysiol*. 2005;45:53–58.
- **30.** Knight AC, Weimar WH. Development of a fulcrum methodology to replicate the lateral ankle sprain mechanism and measure dynamic inversion speed. *Sports Biomech.* 2012;11:402–413.

- **31.** Knight AC, Weimar WH. Effects of previous lateral ankle sprain and taping on the latency of the peroneus longus. *Sports Biomech*. 2012;11:48–56.
- Anderson DL, Sanderson DJ, Hennig EM. The role of external nonrigid ankle bracing in limiting ankle inversion. *Clin J Sport Med.* 1995;5:18–24.
- Beynnon BD, Renstrom PA, Alosa DM, Baumhauer JF, Vacek PM. Ankle ligament injury risk factors: a prospective study of college athletes. J Orthop Res. 2001;19:213–220.
- Chan YY, Fong DTP, Yung PSH, Fung KY, Chan KM. A mechanical supination sprain simulator for studying ankle supination sprain kinematics. J Biomech. 2008;41:2571–2574.
- Cordova ML, Cardona CV, Ingersoll CD, Sandrey MA. Long-term ankle brace use does not affect peroneus longus muscle latency during sudden inversion in normal subjects. J Athl Train. 2000;35:407–411.
- Cordova ML, Ingersoll CD. Peroneus longus stretch reflex amplitude increases after ankle brace application. Br J Sports Med. 2003;37:258–262.
- **37.** Ebig M, Lephart SM, Burdett RG, Miller MC, Pincivero DM. The effect of sudden inversion stress on EMG activity of the peroneal and tibialis anterior muscles in the chronically unstable ankle. *J Orthop Sports Phys Ther.* 1997;26:73–77.
- Eechaute C, Vaes P, Duquet W, Van Gheluwe B. Test-retest reliability of sudden ankle inversion measurements in subjects with healthy ankle joints. J Athl Train. 2007;42:60–65.
- **39.** Eechaute C, Vaes P, Duquet W, Van Gheluwe B. Reliability and discriminative validity of sudden ankle inversion measurements in patients with chronic ankle instability. *Gait Posture*. 2009;30:82–86.
- Eils E, Rosenbaum D. A multi-station proprioceptive exercise program in patients with ankle instability. *Med Sci Sports Exerc.* 2001;33:1991–1998.
- Grüneberg C, Nieuwenhuijzen PH, Duysens J. Reflex responses in the lower leg following landing impact on an inverting and non-inverting platform. *J Physiol.* 2003;550:985–993.
- Hiller CE, Refshauge KM, Beard DJ. Sensorimotor control is impaired in dancers with functional ankle instability. *Am J Sport Med.* 2004;32:216–223.
- Isakov E, Mizrahi J, Solzi P, Susak Z. Response of the peroneal muscles to sudden inversion of the ankle during standing. *Int J Sports Biomech*. 1986;2:100–109.
- 44. Karlsson J, Andreasson GO. The effect of external ankle support in chronic lateral ankle joint instability. *Am J Sports Med.* 1992;20:257–261.
- Kimura IF, Nawoczenski DA, Epler M, Owen MG. Effect of the Air-Stirrup in controlling ankle inversion stress. J Orthop Sports Phys Ther. 1985;9:190–193.
- Konradsen L, Ravn JB. Prolonged peroneal reaction time in ankle instability. Int J Sports Med. 1991;12:290–292.
- 47. Konradsen L, Voigt M, Højsgaard C. Ankle inversion injuries. The role of the dynamic defense mechanism. *Am J Sports Med.* 1997;25:54–58.
- 48. Lofvenberg R, Karrholm J, Sundelin G, Ahlgren O. Prolonged reaction time in patients with chronic lateral instability of the ankle. *Am J Sports Med.* 1995;23:414–417.
- **49.** Lohrer H, Alt W, Gollhofer A. Neuromuscular properties and functional aspects of taped ankles. *Am J Sports Med.* 1999;27:69–75.
- Myers JB, Riemann BL, Hwang JH, Fu FH, Lephart SM. Effect of peripheral afferent alternation of the lateral ankle ligaments on dynamic stability. *Am J Sports Med.* 2003;31:498–506.
- Nieuwenhuijzen PH, Grüneberg C, Duysens J. Mechanically induced ankle inversion during human walking and jumping. *J Neurosci Methods*. 2002;117:133–140.
- Osborne MD, Chou LS, Laskowski ER, Smith J, Kaufman KR. The effect of ankle disk training on muscle reaction time in subjects with a history of ankle sprain. *Am J Sports Med.* 2001;29:627–632.
- **53.** Ottaviani RA, Ashton-Miller JA, Kothari SU, Wojtys EM. Basketball shoe height and the maximal muscular resistance to applied ankle inversion and eversion moments. *Am J Sports Med.* 1995;23:418–423.
- Pederson TS, Ricard MD, Merrill G, Schulthies SS, Allsen PE. The effects of spatting and ankle taping on inversion before and after exercise. *J Athl Train*. 1997;32:29–33.

- **55.** Ricard MD, Sherwood SM, Schulthies SS, Knight KL. Effects of tape and exercise on dynamic ankle inversion. *J Athl Train*. 2000;35:31–37.
- Ricard MD, Schulties SS, Saret JJ. Effects of high-top and low-top shoes on ankle inversion. J Athl Train. 2000;35:38–43.
- Roseubaum D, Becker HP, Gerngro H, Claes L. Peroneal reaction times for diagnosis of functional ankle instability. *Foot Ankle Surg.* 2000;6:31–38.
- Scheuffelen C, Rapp W, Gollhofer A, Lohrer H. Orthotic devices in functional treatment of ankle sprain. Stabilizing effects during real movements. *Int J Sports Med.* 1993;14:140–149.
- Schmitt S, Melnyk M, Alt W, Gollhofer A. Novel approach for a precise determination of short-time intervals in ankle sprain experiments. *J Biomech.* 2009;42:2823–2825.
- 60. Sheth P, Yu B, Laskowski ER, An KN. Ankle disk training influences reaction times of selected muscles in a simulated ankle sprain. *Am J Sports Med.* 1997;25:538–543.
- Shima N, Maeda A, Hirohashi K. Delayed latency of peroneal reflex to sudden inversion with ankle taping or bracing. *Int J Sports Med.* 2005;26:476–480.
- **62.** Ty Hopkins J, McLoda T, McCaw S. Muscle activation following sudden ankle inversion during standing and walking. *Eur J Appl Physiol.* 2007;99:371–378.

- Willems TM, Witvrouw E, Delbaere K, Mahieu N, Bourdeaudhuij ID, Clercq DD. Intrinsic risk factors for inversion ankle sprains in male subjects. Am J Sports Med. 2005;33:415–423.
- **64**. Zhang S, Wortley M, Chen Q, Freedman J. Efficacy of an ankle brace with a subtalar locking system in inversion control in dynamic movements. *J Orthop Sports Phys Ther.* 2009;39:875–883.
- **65.** Mok KM, Fong DTP, Krosshaug T, et al. Kinematics analysis of ankle inversion ligamentous sprain injuries in sports: 2 cases during the 2008 Beijing Olympics. *Am J Sports Med.* 2011;39:1548–1552.
- 66. Fong DTP, Chan YY, Mok KM, Yung PSH, Chan KM. Understanding acute ankle ligamentous sprain injury in sports. *Sports Med Arthrosc Rehabil Ther Technol.* 2009;1:1–14.
- Stormont DM, Morrey BF, An KN, Cass JR. Stability of the loaded ankle. Relation between articular restraint and primary and secondary static restraints. *Am J Sports Med.* 1985;13:295–300.
- **68.** Fong DTP, Ha SCW, Mok KM, Chan CW, Chan KM. Kinematics analysis of ankle inversion ligamentous sprain injuries in sports: five cases from televised tennis competitions. *Am J Sports Med.* 2012;40:2627–2632.